

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
4 April 2002 (04.04.2002)

PCT

(10) International Publication Number  
WO 02/26197 A2

- (51) International Patent Classification<sup>7</sup>: A61K 6/083, 6/09 (72) Inventors: SUN, Benjamin, J.; 3130 Wheatlyn Road, York, PA 17402 (US). LICHKUS, Andrew, M.; 1445 Rosepointe Drive, York, PA 17404 (US).
- (21) International Application Number: PCT/US01/29970
- (22) International Filing Date: 25 September 2001 (25.09.2001) (74) Agents: LOVERCHECK, Dale, R. et al.; Dentsply International Inc., 570 West College Avenue, P.O. Box 872, York, PA 17404-0872 (US).
- (25) Filing Language: English (81) Designated States (*national*): CA, JP.
- (26) Publication Language: English (84) Designated States (*regional*): European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE, TR).
- (30) Priority Data:  
60/670,364 26 September 2000 (26.09.2000) US  
60/237,523 4 October 2000 (04.10.2000) US  
09/682,440 4 September 2001 (04.09.2001) US
- Published:  
— without international search report and to be republished upon receipt of that report
- (71) Applicant: DENTSPLY INTERNATIONAL INC. [US/US]; 570 West College Avenue, P.O. Box 872, York, PA 17405-0872 (US). For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.



WO 02/26197 A2

(54) Title: WAX-LIKE POLYMERIZABLE DENTAL MATERIAL, METHOD AND SHAPED PRODUCT

(57) Abstract: The invention provides high strength dental polymeric dental products made from wax-like polymerizable dental material. These dental products have superior strength compared to products formed from prior wax-like polymerizable materials. Prior wax-like polymerizable materials do not form strong enough polymeric material for making dentures. High strength dentures are made by positioning artificial teeth in wax-like polymerizable dental material of the invention. This material is then shaped and polymerized to the form a denture base of high strength dental polymeric material. These dentures are completed without forming wax and without applying inorganic plaster to the artificial teeth.

## WAX-LIKE POLYMERIZABLE DENTAL MATERIAL, METHOD AND SHAPED PRODUCT

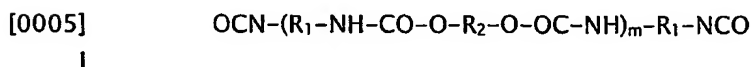
[0001] The invention relates to wax-like polymerizable materials. The invention provides wax-like polymerizable dental materials, and methods of forming dental products of high strength dental polymeric material. *This wax-like polymerizable dental material is quickly and easily reshaped.* It is reshaped by warming, and shaping while warm and then allowing it to cool to room temperature. The shaped wax-like polymerizable dental material is cured to form dental products. These dental products have superior strength compared to products formed from prior wax-like polymerizable materials. Prior wax-like polymerizable materials do not form strong enough polymeric material for making dentures. High strength dentures are made by positioning artificial teeth in wax-like polymerizable dental material of the invention. The disclosures of US patent application Serial Number 09/670,364 filed September 26, 2000 and US provisional patent application Serial Number 06/237,523 filed October 4, 2000 are incorporated herein by reference in their entirety.

[0002] Volkel et al in US Patent 6,057,383 (and Canadian Patent Application 2207351), assigned to Ivoclar, disclose wax-like polymerizable material for making entire dental products. The prior art does not disclose a wax-like polymerizable material for forming dentures or other high strength products.

[0003] The invention provides a high strength dental polymeric material formed from wax-like polymerizable dental material. High strength dental polymeric dental products include partial dentures and full dentures.

[0004] Working wax-like polymerizable dental material, often includes molding, shaping, and/or carving. When heated, wax-like polymerizable dental material softens. In its softened state, it is believed to be partially crystalline and have a flowable amorphous phase, which allows some

flowability of the material. Preferably, wax-like polymerizable dental material is dimensionally stable below 24°C and softened at and above 24-°C. More preferably it is softened at and above 30°C. By heating from its dimensionally stable condition, wax-like polymerizable dental material of the invention undergoes a rapid transition to being freely flowable. By cooling from its softened state, wax-like polymerizable dental material of the invention undergoes a rapid transition to being dimensionally stable. Small volumes of wax-like polymerizable dental material may be worked, while being warmed on the dental device. They may be dispensed from a heated syringe-type dispensing device, spatula, electric spatula, disposal dropper or other mechanical or electrical dispenser. To make a denture, wax-like polymerizable dental material is positioned on a polymeric base plate made from an impression of a patient's mouth. Artificial teeth are positioned in the wax-like polymerizable dental material, which is then shaped by melting and resolidifying. Then the wax-like polymerizable dental material is polymerized to form a denture. Thus the denture is formed without applying inorganic plaster to the artificial teeth and without positioning artificial teeth in a mold as required by conventional lost wax or other similar prior art methods of forming a denture. Compounds, which are readily partially crystallizable and useful in wax-like polymerizable dental material of a preferred embodiment of the invention, include methacrylate (or acrylate) compounds prepared for example by reaction of a urethane pre-oligomer with hydroxylalkylmethacrylate. Preferably such compounds have a structure within the scope of one of general formulas I-V below. Preferably the urethane pre-oligomer is linear, comprises isocyanate end groups and has a structure within the scope of general formula I:



[0006] wherein R<sub>1</sub> and R<sub>2</sub> are either an alkyl having from 1 to 14 carbon atoms or containing at least an aromatic group having from 6 to 14 carbon atoms, m is an integer from 0 to 20, the value of m in the oligomer depends on the molar ratio of diisocyanate to diol used, and the value of m increases as this molar ratio decreases. The diisocyanate portion has the structure OCN-R<sub>1</sub>-NCO and the diol portion has the structure HO-R<sub>2</sub>-OH.

[0007] Alternatively, urethane pre-oligomer is formed by reaction of at least one diol with excess, at least one diisocyanate to yield a urethane

pre-oligomer having a structure within the scope of one or more of general formulas:II-IV

[0008]

### General Formulas:II-IV

$\text{OCN}-(\text{R}_1\text{-NH-CO-O-R}_2\text{-O-OC-NH})_m\text{-(R}_1\text{-NH-CO-O-R}'_2\text{-O-OC-NH)}_n\text{-R}_1\text{-NCO}$	II
$\text{OCN}-(\text{R}_1\text{-NH-CO-O-R}_2\text{-O-OC-NH})_m\text{-(R}''_1\text{-NH-CO-O-R}_2\text{-O-OC-NH)}_n\text{-R}'_1\text{-NCO}$	III
$\text{OCN}-(\text{R}_1\text{-NH-CO-O-R}_2\text{-O-OC-NH})_m\text{-(R}''_1\text{-NH-CO-O-R}'_2\text{-O-OC-NH)}_n\text{-R}'_1\text{-NCO}$	IV

[0009] wherein  $\text{R}_1$ ,  $\text{R}'_1$ ,  $\text{R}_2$  and  $\text{R}'_2$  each independently is an alkyl having from 1 to 14 carbon atoms or at least an aromatic group having from 6 to 14 carbon atoms,  $n$  and  $m$  are each independently integers from 0 to 20, the sum of  $n$  and  $m$  in the oligomer depends on the molar ratio of diisocyanates to diols used, and the value of the sum of  $n$  and  $m$  increases as this molar ratio decreases. The diisocyanates have the structures  $\text{OCN-R}_1\text{-NCO}$  and  $\text{OCN-R}'_1\text{-NCO}$  and the diols have the structures  $\text{HO-R}_2\text{-OH}$  and  $\text{HO-R}'_2\text{-OH}$ . The more complex structures of urethane pre-oligomer are constructed from at least two different diols and at least two different diisocyanates.

[0010] Reaction of the urethane pre-oligomer with the ethylenically unsaturated monomer as defined below yields a polymerizable compound having the structure within the scope of the general formula  $\text{V:CH}_2=\text{C}(\text{R}_3)\text{-CO}_2\text{-R}_4\text{-CO-NH-(R}_1\text{-NH-CO-O-R}_2\text{-O-OC-NH)}_n\text{-R}_1\text{-NH-CO-R}_4\text{-O}_2\text{C-C}(\text{R}_3\text{-})=\text{CH}_2$  V wherein  $\text{R}_3$  is hydrogen, or an alkyl, such as a methyl group, and  $\text{R}_4$  is an alkyl group having from 1 to 14 carbon atoms, and  $n$  is an integer from 0 to 20. The typical ethylenically unsaturated monomer is a hydroxyalkyl (meth) acrylate, e.g. 2-hydroxyethyl methacrylate, hydroxypropyl methacrylate, caprolactone 2-(methacryloyloxy) ethyl ester, etc.

[0011] Preferred mechanical properties of cured resin and the adequate handling properties of compositions, polymerizable compound, are present when the value of  $n$  in the compound is not greater than 10; more preferably  $n$  is not greater than 5. The preferred value of  $n$  in the compound largely depends on the requirements of the specific

application. The most preferable value of  $n$  in the compound for aromatic ring based diol is between 1 and 3. Therefore, the molar ratio of diisocyanate to diol for aromatic ring based diol is most preferable between 1.33 and 2. The most preferable value of  $n$  in the compound for alkyl based diol is between 1 and 4. Therefore, the molar ratio of diisocyanate to diol for alkyl based diol is most preferable between 1.25 and 2.

[0012] Catalysts known in the art may be used to accelerate the formation of the isocyanate-ended pre-oligomer and end-capped ethylenically unsaturated monomer, for examples, tertiary amines and metal salts, e.g. stannous octoate and in particular dibutyl tin dilaurate. Preferred stabilizers used in this invention are butylated hydroxytoluene (BHT) and the methyl ether of hydroquinone (MEHQ).

[0013] Preferably compounds of the invention are difunctional methacrylates including reaction products of bisphenol A propoxylate, 1,6-diisocyanatohexane and 2-hydroxyethyl methacrylate, reaction products of bisphenol A propoxylate, trimethyl-1, 6-diisocyanatohexane and 2-hydroxyethyl methacrylate, a series of reaction products of bisphenol A, trimethyl-1, 6-diisocyanatohexane and 2-hydroxyethyl methacrylate, a series of reaction products of bisphenol A, 1,6-diisocyanatohexane and 2-hydroxyethyl methacrylate, a series of reaction products of trimethyl-1,6-diisocyanatohexane, 2,5-dimethyl-2,5-hexanediol and 2-hydroxyethyl methacrylate, a series of reaction products of trimethyl-1,6-diisocyanatohexane, 1,6-diisocyanatohexane, 2,5-dimethyl-2,5-hexanediol and 2-hydroxyethyl methacrylate, a series of reaction products of trimethyl-1,6-diisocyanatohexane, 1,6-diisocyanatohexane, bisphenol A propoxylate and 2-hydroxyethyl methacrylate, caprolactone 2-(methacryloyloxy)ethyl ester, and derivatives of above compounds.

[0014] Diisocyanates useful for making wax-like polymerizable dental material of the invention include trimethyl-1,6-diisocyanatohexane, 1,6-diisocyanatohexane, 1,8-diisocyanatooctane, isophorone diisocyanate, 4,4"-methylenebis(cyclohexyl isocyanate), cyclohexyl diisocyanate, 3-methylhexane-1, 6-diisocyanate, 3-ethyl-1,6-hexanediisocyanate, 5-methyl-1,9-nonanediisocyanate, 5-ethyl-1,10-decanediisocyanate, 2,3-dimethyl-1,6-hexanediisocyanate, 2,4-dimethyl-1,8-octanediisocyanate, 2,4,6-trimethyl-1,7-heptanediisocyanate, 2,3-dimethyl-5-ethyl-1,8-octanediisocyanate, 2-methyl-4,6,8,10-tetrapropyl-1,12-

dodecanediisocyanate and the like, and mixtures thereof. Examples of diisocyanates that are also suitable include aromatic diisocyanates, for example, 4,4'-methylene bis(phenyl isocyanate), 2,4-tolylene diisocyanate, 2,6-tolylene diisocyanate, 1,4-phenyl diisocyanate, 1,5-naphthalene diisocyanate, 1,3-bis (isocyanatomethyl)benzene, 1,3-bis(isocyanato-1-methylethyl)benzene, 1,3-bis(isocyanatomethyl)cyclohexane, 3,3'-bitoluene diisocyanate, 1,4-xylene diisocyanate and the like, and mixtures thereof.

[0015] Examples of diols useful for making compounds for wax-like polymerizable dental material of the invention include 1,4-butanediol, 1,6-hexanediol, 1,10-decanediol, 1,9-decanediol, 1,12-dodecanediol, 1,14-tetradecanediol, 2,5-dimethyl-2,5-hexanediol, hydrogenated bisphenol A, bisphenol A, propoxylated bisphenol A, ethoxylated bisphenol A, bis (2-hydroxyethyl) terephthalate, and mixtures thereof.

[0016] Examples of methacrylates (or acrylates) useful for making compounds for wax-like polymerizable dental material of the invention include 2-hydroxyethyl methacrylate, 2-hydroxyethyl acrylate, 2-hydroxypropyl methacrylate, 3-hydroxypropyl methacrylate, hydroxypropyl acrylate, glycerol dimethacrylate, glycerolmonomethacrylate, 2-hydroxyethyl acrylate, hydroxypropyl acrylate, 4-hydroxybutyl methacrylate, 4-hydroxybutyl acrylate, 2-hydroxy-3-phenoxypropyl acrylate, 2-hydroxycyclohexyl methacrylate, caprolactone 2-(methacryloyloxy)ethyl ester, pentaerythritol triacrylate, 2-hydroxycyclohexyl acrylate and mixture thereof.

[0017] Wax-like polymerizable dental material may include one or more initiating systems to cause them to harden promptly. Light curable wax-like polymerizable dental materials preferably include a light sensitizer, for example camphorquinone, Lucirin TPO, or methyl benzoin which causes polymerization to be initiated upon exposure to activating wavelengths of light; and/or a reducing compound, for example tertiary amine.

[0018] A room temperature or heat activating catalyst system is preferably included in the wax-like polymerizable dental material of the invention. Preferably included is a peroxide capable of producing free radicals when activated by a reducing agent at room temperature or by heating. Preferred peroxides include benzyl peroxide and lauroyl peroxide.

[0019] Wax-like polymerizable dental materials of the invention are believed to rapidly partially recrystallize. This rapid recrystallizability provides a unique combination of free flowability and dimensional stability, depending on its temperature. It is believed that the material rapidly transitions from a freely flowable state by means of rapid crystallization to a dimensionally stable state. The material at solidification temperatures is partially crystalline and the crystallinity present in an amorphous phase results in the effective dimensional stability of the material. "Crystallinity" as used herein refers to regularity and order within a material resulting in a heat of fusion of at least 1.0 J/g at and below 50°C. Heat of Fusion as used herein refers to enthalpy of fusion as determined by ASTM 793-95. Percent crystallinity is determined by measuring the heat of fusion using differential scanning calorimetry according to ASTM test method E 793-95.

[0020] The wax-like polymerizable dental material of the invention is useful for formation of dental products including full dentures, partial dentures, denture liners, custom trays, artificial teeth, repairs for natural teeth, veneers, denture repairs, denture relines, night guards, splints, retainers, orthodontic components, crowns, bridges, provisional dental devices, inlays, onlays, and tooth restorative fillings, orthodontic appliances, oral orthopedic appliances, temporary dentures, temporary partial dentures; maxillofacial prostheses, obturators, and ocular prostheses.

[0021] Compositions in accordance with the invention may further include fillers, pigments, stabilizers, plasticizers and fibers. Preferably, polymerizable dental compositions in accordance with the invention include from about 2 to about 95 percent by weight filler particles. More preferably, these compositions include from about 10 to about 85 percent by weight filler. Nanocomposites and ceramers may be formed from these composites. The fillers preferably include both organic and inorganic particulate fillers to further reduce polymerization shrinkage, improve wear resistance and modify the mechanical and physical properties.

[0022] A preferred embodiment of the invention provides a high strength dental polymeric material formed by light curing wax-like polymerizable dental material shaped into at least a portion of a denture base. Preferably the wax-like polymerizable dental material has a flexural modulus of at least 400,000 psi and a flexural strength of at least 7,000

psi and an un-notched impact strength of at least 2 foot-pounds/inch. Preferably the denture comprises denture base, and a tooth comprising an interpenetrating polymer network polymeric matrix and at least 0.1 percent by weight of self-lubricating particles having a particle size less than 500 microns effectively bonded to and distributed in the polymeric matrix. Preferably the bond strength between the tooth and the denture base is at least 4,480 psi.

[0023] "Wax-like" as used herein refers to material which is flowable (fluid) above 40°C, and becomes dimensionally stable (solidifies: i.e. is nonfluid) at least at and below 23°C, within 5 minutes. Thus, wax-like material is flowable when it is at and above 40°C, and becomes dimensionally stable when it is at and below 23°C. Flowable wax-like material having a temperature from 100°C to 40°C, becomes dimensionally stable within 5 minutes by cooling by exposure to an ambient temperature between 23 °C and 0°C. Flowable wax-like material having a temperature from 100°C to 40°C, becomes dimensionally stable within (in order of increasing preference) 2, 1, 0.5 or 0.3 minutes by cooling by exposure to an ambient temperature between 23 °C and 0°C.

[0024] "High strength dental polymeric material" as used herein refers to material having a polymeric matrix having a flexural modulus of at least 250,000 psi and a flexural strength of at least 5,000 psi. Optionally, high strength dental polymeric material includes reenforcing filler. However, the polymeric matrix alone (without any reenforcing filler) has a flexural modulus of at least 250,000 psi and a flexural strength of at least 5,000 psi. Preferably high strength dental polymeric material has a polymeric matrix having a flexural modulus of at least 300,000 psi and a flexural strength of at least 7,000 psi, and an un-notched impact strength of at least 2 foot-pounds/inch<sup>2</sup>. More preferably high strength dental polymeric material in order of increasing preference has a polymeric matrix having a flexural modulus of at least 350,000 psi and a flexural strength of at least 12,000 psi, and an un-notched impact strength of at least 3.0 foot-pounds/inch. High strength dental polymeric material is preferably formed into dental products including full dentures, partial dentures, denture relines, night guards, crowns and bridges by polymerization of wax-like polymerizable dental material.

[0025] "Flexural strength, and flexural modulus" as used herein refers to results of testing according to ASTM D790 (1997). "Notched impact



strength" as used herein is also referred to as "notched Izod impact resistance" and refers to results of testing according to ASTM D256 (1997). "Un-notched impact strength" as used herein refers to results of testing according to ASTM D4812 (1993).

[0026] In the following examples, unless otherwise indicated, all parts and percentages are by weight; Lucirin TPO refers to 2,4,6-trimethylbenzoyldiphenylphosphine oxide made by BASF, and the visible light curing unit used was a TRIAD VLC visible light curing unit modified by adding a fifth light to provide about 30 milliwatts/cm<sup>2</sup> of from 350 to 450 nm light.

[0027] Example 1 Preparation of Oligomer

[0028] A reactor was charged with 1176 grams of trimethyl-1,6-diisocyanatohexane (5.59 mol) and 1064 grams of bisphenol A propoxylate (3.09 mol) under dry nitrogen flow and heated to about 65°C under a positive nitrogen pressure. To this reaction mixture, 10 drops of catalyst dibutyltin dilaurate were added. The temperature of the reaction mixture was maintained between 65°C and 140°C for about 70 minutes and followed by additional 10 drops of catalyst dibutyltin dilaurate. A viscous paste-like isocyanate end-capped intermediate product was formed and stirred for 100 minutes. To this intermediate product, 662 grams (5.09 mol) of 2-hydroxyethyl methacrylate and 7.0 grams of BHT as an inhibitor were added over a period of 70 minutes while the reaction temperature was maintained between 68°C and 90°C. After about five hours stirring under 70°C, the heat was turned off, and oligomer was collected from the reactor as semi-translucent flexible solid and stored in a dry atmosphere.

[0029] Example 2 Preparation of Monomer

[0030] A reaction flask was charged with 700 grams of 1,6-diisocyanatohexane and heated to about 70°C under a positive nitrogen pressure. To this reactor were added 1027 grams of 2-hydroxyethyl methacrylate, 0.75 gram of catalyst dibutyltin dilaurate and 4.5 grams of butylated hydroxy toluene (BHT). The addition was slow and under dry nitrogen flow over a period of two hours. The temperature of the reaction mixture was maintained between 70°C and 90°C for another two hours and followed by the addition of 8.5 grams of purified water. One hour later,

the reaction product was discharged as clear liquid into plastic containers and cooled to form a white solid and stored in a dry atmosphere.

[0031]            Example 3. Preparation of Polymerizable Denture Contour Material

[0032]            A wax-like polymerizable dental material was prepared by stirring at 85°C a liquid mixture of 63.0 grams of oligomer made the procedure of Example 1 and 37.0 grams of compound of Example 2. 0.35 gram of 2,4,6- trimethylbenzoyldiphenylphosphine oxide, (Lucirin TPO made by BASF), 0.5 gram of solution containing 8.3% camphorquinone (CQ), 25% ethyl 4- dimethylaminobenzoate (EDAB) and 66.7% 1,6-hexanediol dimethacrylate (HDDMA).

[0033]            Example 4 Preparation of Polymerizable Denture Base Plate (or Reline) Material

[0034]            A light curable polymerizable material was prepared by stirring at 85°C a liquid of 98.0 grams of TBDMA oligomer of Example 1, 0.35 gram of 2,4,6- trimethylbenzoyldiphenylphosphine oxide, (Lucirin TPO made by BASF), 1.5 gram of solution containing 8.3% camphorquinone (CQ), 25% ethyl 4- dimethylaminobenzoate (EDAB) and 66.7% 1,6-hexanediol dimethacrylate (HDDMA), 0.1 gram of red acetate fibers and 0.05 gram of pigment.

[0035]            Example 5 Preparation of Polymerizable wax-like Denture Contour Material

[0036]            A light curable wax-like polymerizable dental material was prepared by stirring at 85°C a liquid mixture of 50.5 grams of oligomer of Example 1, 45.0 grams of monomer of Example 2 and 4.0 grams of stearyl acrylate from Sartomer. To this mixture were added 0.35 gram of 2,4,6- trimethylbenzoyldiphenylphosphine oxide (Lucirin TPO), 0.1 gram of red acetate fibers and 0.05 gram of pigment concentrates. The polymerizable wax-like material formed becomes flowable at 65 to 68 °C.

[0037]            Example 6 Preparation of Polymerizable Denture Set-up Material

[0038]            A light curable polymerizable material was prepared by stirring at 85°C a liquid mixture of 84.5 grams of oligomer of Example 1 and 15.0 grams of monomer of Example 2. To this mixture, 0.35 gram of 2,4,6-

trimethylbenzoyldiphenylphosphine oxide (Lucirin TPO), 0.1 gram of red acetate fibers and 0.05 gram of pigment were added.

[0039]           Example 7 Preparation of a Denture without Forming a Mold Cavity of a Denture Base.

[0040]           A plaster cast of a patient's mouth is coated with a release agent (e.g., Al-Cote and Isolant sold by Dentsply International Inc. or Teflon solution such as Krytox from Dupont) and heated to 55°C in an incubator. An arch-shaped baseplate resin containing 14 grams of the product of Example 4 is applied and shaped onto the warm cast. The resin is shaped and flowed to fully cover the cast, using finger pressure and trimming to form a baseplate. The baseplate is cured for 10 minutes in the visible light curing unit. A sufficient quantity of the product of Example 6 is formed into a rope. The rope is applied to the baseplate. Then artificial teeth are pressed into the rope with the thickness of the rope adapted to adequately cover the appropriate surfaces of the teeth to provide support. Melted product of Example 5 from an about 87°C wax pot is applied by using an electric spatula between the teeth and the baseplate to fully embed teeth and to flow into fissures between teeth and to smooth the outer surface of the denture. Hot air from a small nozzle hot air gun may also be applied to let the product of Example 5 flow into fissures between teeth and smooth the outer surface of the denture. The lingual and buccal surfaces of the denture are contoured, trimmed and carved using a spatula. The denture is placed in a patient's mouth for try-in at a dental office and tooth positions are adjusted. The denture back is fitted to the cast and the TRIAD Air Barrier Coating is painted on the denture. Then a model release agent (MRA) sold by Dentsply International Inc. is applied to around posterior teeth and supporting resin. A strip of Triad gel is applied on surface between teeth and supporting resin to form a continuous circle and cured in a visible light curing unit for 10 minutes, followed by post curing for 8 hours of gradually cooling to 23°C. When cured, the denture is washed with water to remove all traces of Air Barrier Coating. The denture is then finished and polished.

[0041]           Example 8 Preparation of a Partial Denture without Forming a Mold Cavity (investment) of a Denture Base

[0042]           A removable partial denture framework is fabricated. A separating medium is applied to a gypsum cast of the patient's dentition.

A sufficient quantity of the product of Example 4 is applied onto the edentulous areas of the cast and adapted with finger pressure or appropriate instruments. Excess material is trimmed with a hot spatula. A sufficient quantity of the product of Example 4 is adapted into the tissue side finish line of the partial denture framework. The framework is seated on the cast firmly, embedding the uncured material of Example 4. All rests and tissue stops are varnished as correctly positioned on the cast, indicating that the framework is fully seated. Excess material is removed and these baseplate areas are cured in the visible light curing unit. A rope of the product of Example 6 is adapted onto the precured baseplate/edentulous areas. The rope has a thickness sufficient to cover the ridge lap surfaces of the teeth to provide support for the teeth and to seat the teeth, which are then set up in the rope. A portion the product of Example 5 is applied between the teeth and the baseplate. A small nozzle hot air gun is used to melt the product of Example 5 so that it flows into the fissures between teeth as the outer surface smoothes. The lingual and buccal surfaces of the edentulous areas are contoured, trimmed and carved using an electric hot spatula, sharp tools and hot air gun. The partial denture wax-up is removed from the cast for try-in. The denture is placed in a patient's mouth for try-in at a dental office and tooth positions adjusted if needed. The partial denture is fitted to a modified cast (reduced soft tissue heights of contour). TRAID Air Barrier Coating is painted onto the denture. Then a mold release agent (MRA) sold by Dentsply International, Inc. is applied around the posterior teeth and supporting resin. A strip of triad gel is applied between teeth and on the surface of the supporting resin to form a continuous circle. The denture is then cured in the visible light curing unit for 10 minutes, followed by cooling over a 2 hour period to 23°C. When cured, the partial denture is washed with water to remove all traces of Air Barrier Coating. The partial denture is then finished and polished.

[0043]            Example 9. Preparation Of A Night Guard Without Forming A Mold Cavity Of A Night Guard.

[0044]            A plaster cast of a patient's teeth is coated with a release agent. 20 grams of the product composition of Example 3 is applied over the release agent and warmed to 50°C in an oven. The composition is shaped using finger pressure and trimming to form a night guard which hardens when cooling to room temperature. The surfaces of the night guard are contoured, trimmed and carved using an electric hot spatula and hot air gun. After the night guard is examined and adjusted to fit articulator, the

night guard is fitted to the cast and a TRAID Air Barrier Coating is painted on the denture and cured for 10 minutes. The clear night guard is then washed with water to remove all traces of Air Barrier Coating. The night guard is then finished and polished.

[0045] Example 7B of US Patent 6,057,383 (and Canadian Patent Application 2207351) was followed and the polymeric product thereof was tested to provide the information in the following Table. The polymerizable wax-like material of the present invention made by following the procedure of Example 5 was polymerized and the polymeric product was tested to provide the information in the following Table. Comparing the test results, Example 5's flexural strength is more than 500 percent greater than that of the tested material of US Patent 6,057,383. Example 5 of the present invention has a flexural modulus which is more than two times greater than that of the polymerizable wax-like material of US Patent 6,057,383. Example 5 of the present invention has an un-notched Impact Strength which is more than eight times greater than that of the polymerizable wax-like material of US Patent 6,057,383. Example 5 of the present invention has a notched Impact Strength which is more than two times greater than that of the polymerizable wax-like material of US Patent 6,057,383. Overall results show that the material of the invention is suitable for making a denture while the flexural strength and un-notched impact strength of the comparative examples are insufficient.

[0046]

TABLE: COMPARISON OF POLYMERIZABLE WAX-LIKE MATERIALS

	Flexural strength(psi)	Flexural Modulus (kpsi)	Un-notched Impact Strength (ft-lbf/in)	Notched Impact Strength (ft-lbf/in <sup>2</sup> )
US Patent 6,057,383 (Ivoclar) Example 7B	2897	207.9	0.51	0.53
Example 5 of the present invention	16820	446.5	4.45	1.28

[0047] It should be understood that while the present invention has been described in considerable detail with respect to certain specific embodiments thereof, it should not be considered limited to such embodiments but may be used in other ways without departure from the spirit of the invention and the scope of the appended claims.

## Claims

[c1]

A method, comprising: polymerizing a wax-like polymerizable dental material to form a high strength dental polymeric material.

[c2]

The method of Claim 1 wherein said high strength dental polymeric material is at least a portion of a full denture, partial denture, night guard or bridge.

[c3]

The method of Claim 1 wherein said wax-like polymerizable dental material is shaped into at least a portion of a denture base and said polymeric material has an un-notched impact strength of at least 2 foot-pound/inch.

[c4]

The method of Claim 1 wherein said wax-like polymerizable dental material is shaped into at least a portion of a denture base.

[c5]

The method of Claim 1 further comprising light curing said wax-like polymerizable dental material.

[c6]

The method of Claim 1 further comprising shaping wax-like polymerizable dental material to form a dental product.

[c7]

The method of Claim 6 wherein said wax-like polymerizable dental material is shaped into at least a portion of a denture base and said high strength dental polymeric material has flexural modulus of at least 300,000 psi and a flexural strength of at least 7,000 psi and an un-notched impact strength of at least 4 foot-pounds/inch.

[c8]

A high strength dental polymeric material formed from wax-like polymerizable dental material.

[c9]

The material of Claim 8 wherein said wax-like polymerizable dental material is shaped into at least a portion of a denture base and said high strength dental polymeric material is formed by light curing and has an un-notched impact strength of at least 2 foot-pound/inch.

[c10]

The material of Claim 8 wherein said wax-like polymerizable dental material is shaped into at least a portion of a denture base and said polymeric material has flexural modulus of at least 400,000 psi and a flexural strength of at least 7,000 psi and an un-notched impact strength of at least 2 foot-pounds/inch.

[c11]

The material of Claim 8 wherein said wax-like polymerizable dental material is shaped into at least a portion of a night guard or a denture base.

[c12]

The material of Claim 8 wherein said polymeric material has an un-notched impact strength of at least 2 foot-pound/inch.

[c13]

The material of Claim 8 wherein said wax-like polymerizable dental material is shaped into at least a portion of a full denture, partial denture, denture liner, custom tray, artificial teeth, veneer, denture reline, night guard, splint, retainer, orthodontic component, crown, bridge, provisional dental device, inlay, onlay, orthodontic appliance, oral orthopedic appliance, temporary denture, temporary partial denture; maxillofacial prosthesis, obturator, or ocular prosthesis.

[c14]



The material of Claim 13 wherein said polymeric material has an un-notched impact strength of at least 2 foot-pound/inch.

[c15]

The material of Claim 13 wherein said polymeric material has a flexural modulus of at least 300,000 psi, and flexural strength of at least 7,000 psi.

[c16]

The material of Claim 8 wherein said polymeric material has an un-notched impact strength of at least 2 foot-pound/inch, a flexural modulus of at least 300,000 psi, and flexural strength of at least 7,000 psi.

[c17]

A denture having denture base and at least one artificial tooth, said denture base comprising high strength dental polymeric material formed from wax-like polymerizable dental material.

[c18]

The denture of Claim 17 wherein said denture is a partial denture or a full denture.

[c19]

The denture of Claim 17 wherein said polymeric material has an un-notched impact strength of at least 2 foot-pound/inch.

[c20]

The denture of Claim 17 wherein said polymeric material has a flexural modulus of at least 300,000 psi, and flexural strength of at least 7,000 psi.

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
4 April 2002 (04.04.2002)

PCT

(10) International Publication Number  
**WO 02/026197 A3**

- (51) International Patent Classification<sup>7</sup>: **A61K 6/09, 6/083** (74) Agents: **LOVERCHECK, Dale, R. et al.**; Dentsply International Inc., 570 West College Avenue, P.O. Box 872, York, PA 17404-0872 (US).
- (21) International Application Number: **PCT/US01/29970**
- (22) International Filing Date: 25 September 2001 (25.09.2001) (81) Designated States (*national*): CA, JP.
- (25) Filing Language: English (84) Designated States (*regional*): European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE, TR).
- (26) Publication Language: English
- (30) Priority Data: Published:  
— with international search report
- |            |                                |    |  |
|------------|--------------------------------|----|--|
| 60/670,364 | 26 September 2000 (26.09.2000) | US | (88) Date of publication of the international search report: |
| 60/237,523 | 4 October 2000 (04.10.2000)    | US | 14 August 2003   |
| 09/682,440 | 4 September 2001 (04.09.2001)  | US |  |

(71) Applicant: **DENTSPLY INTERNATIONAL INC.**  
[US/US]; 570 West College Avenue, P.O. Box 872, York,  
PA 17405-0872 (US).

*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*

(72) Inventors: **SUN, Benjamin, J.**; 3130 Wheatlyn Road,  
York, PA 17402 (US). **LICHKUS, Andrew, M.**; 1445  
Rosepointe Drive, York, PA 17404 (US).



**WO 02/026197 A3**

(54) Title: **WAX-LIKE POLYMERIZABLE DENTAL MATERIAL, METHOD AND SHAPED PRODUCT**

(57) Abstract: The invention provides high strength dental polymeric dental products made from wax-like polymerizable dental material. These dental products have superior strength compared to products formed from prior wax-like polymerizable materials. Prior wax-like polymerizable materials do not form strong enough polymeric material for making dentures. High strength dentures are made by positioning artificial teeth in wax-like polymerizable dental material of the invention. This material is then shaped and polymerized to the form a denture base of high strength dental polymeric material. These dentures are completed without forming wax and without applying inorganic plaster to the artificial teeth.

A. CLASSIFICATION OF SUBJECT MATTER  
IPC 7 A61K6/09 A61K6/083

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 6 057 383 A (FISCHER KARL ET AL) 2 May 2000 (2000-05-02) cited in the application column 2, line 37 - line 40 column 4, line 39 - line 58 claims; table 2	1,2,4-6, 8,9,11, 13,17,18
Y		1-20
Y	EP 0 630 640 A (DENTSPLY INT INC) 28 December 1994 (1994-12-28) page 5, line 54 -page 6, line 14 page 6, line 55 -page 8, line 48 examples; table 2	1-20

-/--

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

\* Special categories of cited documents :

- \*A\* document defining the general state of the art which is not considered to be of particular relevance
- \*E\* earlier document but published on or after the international filing date
- \*L\* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- \*O\* document referring to an oral disclosure, use, exhibition or other means
- \*P\* document published prior to the international filing date but later than the priority date claimed

- \*T\* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- \*Y\* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- \*Z\* document member of the same patent family

Date of the actual completion of the international search

22 May 2002

Date of mailing of the international search report

31/05/2002

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

Authorized officer

Cousins-Van Steen, G

## INTERNATIONAL SEARCH REPORT

Int lonal Application No

PCT/US 01/29970

## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	<p>MOSZNER N ET AL: "SYNTHESIS, CHARACTERIZATION AND POLYMERIZATION OF WAXY MONOMERS" ANGEWANDTE MAKROMOLEKULARE CHEMIE. APPLIED MACROMOLECULAR CHEMISTRY AND PHYSICS, WILEY VCH, WEINHEIM, DE, vol. 245, 1 March 1997 (1997-03-01), pages 155-164, XP000692240 ISSN: 0003-3146</p> -----	

# INTERNATIONAL SEARCH REPORT

Information on patent family members

Int onal Application No

PCT/US 01/29970

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
US 6057383	A	02-05-2000	DE 19626356 A1	02-01-1998
			CA 2207351 A1	18-12-1997
			EP 0813856 A2	29-12-1997
			JP 3151420 B2	03-04-2001
			JP 10059815 A	03-03-1998
			JP 2000186011 A	04-07-2000
EP 0630640	A	28-12-1994	US 5502087 A	26-03-1996
			AU 6477294 A	05-01-1995
			AU 6477394 A	05-01-1995
			CA 2124426 A1	24-12-1994
			CA 2126541 A1	24-12-1994
			DE 69426093 D1	16-11-2000
			DE 69426093 T2	10-05-2001
			EP 0630640 A1	28-12-1994
			EP 0630641 A1	28-12-1994
			ES 2152276 T3	01-02-2001
			JP 7145017 A	06-06-1995
			JP 7145018 A	06-06-1995
			US 5554665 A	10-09-1996